

STRESS ANALYSIS OF TWO DIFFERENT ATTACHMENTS FOR A SINGLE IMPLANT RETAINED MANDIBULAR OVERDENTURES IN THE MIDLINE (IN VITRO STUDY)

Ahmed H. M. Rashad* , Hamdi Abo Alfotouh Hamed ** and Nouran Mahmoud Abdel Nabi ***

ABSTRACT

Objective: aiming to record the induced micro-strain around one installed implant in the midline of a completely edentulous mandible using strain gauges utilizing an implant retained overdenture with two different types of attachments Ball and CMLOC attachment.

Materials and methods: An acrylic resin test resin test model representing a completely edentulous lower arch was used. The distal part of the residual ridge was covered with silicon based soft liner to stimulate the mucoperiosteum. Steps of complete denture fabrication was followed in conventional manner. Duplication of the finished denture was carried out to be used as a surgical stent. A single implant installed in the midline. After the implant was installed in the acrylic resin cast, the ball attachment was screwed to the implant. The denture was prepared for the direct pick up procedure, the same procedure repeated for CM IOC attachment. Four strain gauges around were installed on all surfaces of implant (Buccal. Lingual. Mesial .Distal) to monitor the effect of the applied loads vertical on the two types of attachments. A vertically load applied of 100 N static load was applied by using universal testing machine at two different sites (unilateral left first molar and bilaterally).

Results : When the load applied unilaterally on the left side ,it was shown that the single implant retained overdenture with the Ball attachment has shown higher microstrain than the CMLOC ,average microstrain for Ball (391.26) N , and for CMLOC (223.22) N . When the load applied bilaterally, the single implant retained overdenture with the CMLOC (269.05)N attachment has shown higher microstrain than the Ball (106.79) N.

Conclusion: It can be concluded from this invitro study that the newly introduced attachment the CMLOC lends to show a better performance with regards to the micro-strains induced around the implants . On the other hand the Ball attachments tends to show more micro-strain around the implants.

* Oral Implantology Department, Faculty of Dentistry Cairo University, Egypt

** Removable Prosthodontics Department, Faculty of Dentistry Cairo University, Egypt

INTRODUCTION

Severe atrophy of the alveolar process and underlying basal bone often results in several problems with mandibular denture. These problems include insufficient retention of the lower denture, intolerance to loading by the mucosa, pain, difficulties with eating and speech, loss of soft tissue support, altered facial appearance and reduced quality of life in this specific patient group. These problems are a challenge for the prosthodontist and surgeon^(1,2).

There are several types of attachment that can be used to retain an implant over denture, they are mainly classified into splinted attachments such as bar attachments or un-splinted attachments such as ball or locator attachment. The un-splinted attachments have been more commonly used than the splinted attachment owing to the smaller space requirements within the prosthesis, ease of cleaning, more economical, and lower sensitivity to techniques^(3,4).

Ball and socket attachment has been the most popular un-splinted attachment to retain a mandibular overdenture, because its simplicity and cost effectiveness. A newly introduced attachment made from polyetherketoneketone (PEKK) which is a member of the polyaryletherketones (PAEKs). Polyaryletherketones have the advantage of high chemical and mechanical resistance to wear and high tensile, fatigue and flexural strengths. According to the manufacturer Cendres and Metaux, Polyetherketoneketone has 80% higher compressive strengths than other PAEK materials⁽⁵⁾.

Excessive stresses transmitted to the underlying bone can result in bone resorption consequently resulting in implant failure. The distribution of stresses around an implant would depend upon many factors such as; implant design and diameter,

abutment length, angulation, and its relation with the implant platform^(6,7).

Various methods have been used to analyze the transmission of stresses to the underlying bone among them are; photo elastic, strain gauge and finite element analysis. Photo elastic analysis is of low cost, it's a simple method, and it provides a qualitative analysis of the stresses present in the bone but doesn't allow an accurate measurement⁽⁸⁾.

There has been a major controversy in the literature to the number of implants required to support an overdenture, 4, 3, 2 or even a single implant in the midline to improve function and esthetics of the patient. A single implant retained overdenture has proved to be a reliable and cost effective treatment option for elderly patient^(9,10).

The question now arises for a single implant retained mandibular overdenture, which attachment will induce the minimum microstrain to the underlying implant?

AIM OF THIS STUDY

The aim of this in vitro study is to compare the induced micro-strain for a single implant retained mandibular overdenture with two different types of attachments Ball and CMLOC attachment.

MATERIALS AND METHODS:

Acrylic model construction:

An acrylic resin model was fabricated from a mandibular completely edentulous simulating a clinical condition. Acrylic model was fabricated according to the following steps; A final impression **Fig. (1)** using silicon impression material* of completely edentulous ridge was recorded then molten wax was then poured into the impression to produce a wax cast. After wax hardening inspection for any discrepancy was adjusted*. The waxed cast

* Elite dental stones Zhermack- BadiaPolesine (Rovigo)-Italy.



Fig. (1): Final impression using silicon impression material

was then flaked and wax elimination was carried out. The created mold was packed with heat polymerized acrylic resin, and then cured by using long curing cycle 8 hours at 70°C. The flask was left to bench cool for two hours before deflasking, the model is finished and polished** Fig. (2).

Simulation of the artificial mucosa:

An index of the acrylic completely edentulous cast was made using putty impression material. The posterior ridge distal to the second premolar was modified by reducing the distal area of the crest of the ridge using a round bur on the buccal and



Fig. (2): Acrylic resin model

lingual surfaces then the soft molloplast B was used to reline the reduced area. The reduced edentulous area was painted by adhesive*** before application of molloplast B Fig.(3) . The index wax then used for the molloplast B that to cover the ridge.

Implant installation :

The lower finished denture was then duplicated



Fig. (3): Application of soft molloplast B

into an acrylic resin stent. This stent would be used as a surgical stent to guide for implant installation .The stent was then modified by placing holes around central incisor area. Drilling was carried out by using a round bur, then the midline was identified by the initial drill, then intermediate drill and then final drill was 3.7 mm for implant* size (3,9 X10) mm. length of drilling was identified by graduation of the drill.

The implant was the attached to the surveyor Fig. (4) Corresponding to the drilled hole, and then a mix of self cure acrylic resin was added to the drill hole, and then the implant was placed.

* Acrostone-Heat polymerized denture base material-England

** Putty c-silicone impression material Zermack-Badiapolesine (Rovigo)-Italy.

*** Primo, DETAX, Voco, 3002-Germany

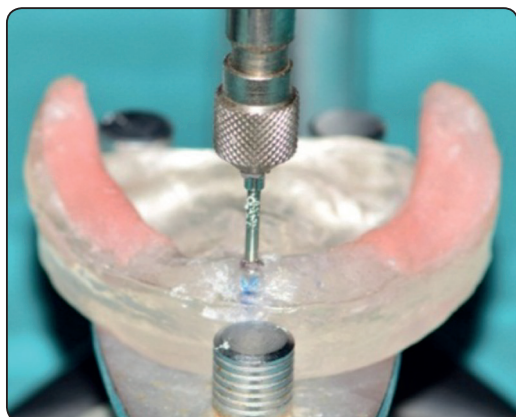


Fig. (4): Implant attached to the surveyor



Fig. (5) : Strain gauges around the implant

The pick up:

After the implant was installed in the acrylic resin cast, the ball attachment of (group 1) (**Mandibular overdenture retained with Ball abutment**) was screwed to the implant. A mix of auto polymerized acrylic resin was then applied on the fitting surface of the denture opposite to the abutment. The denture base was then seated on the model and the attachment, then after complete setting of the acrylic resin, the denture with the housing and nylon cap in the fitting surface was finished and polished

Preparation of the model for installation of the strain gauges:

The preparation was of a box shape with a thickness of 1mm of acrylic resin around the implant, having four prepared surfaces; Buccal (B), Lingual (L), Mesial (M), and Distal (D) **Fig. (5)**. The four prepared surfaces had to be flat and parallel to the long axis of the implant each prepared surface had to be smoothed using sand paper before installation of the strain gauges to avoid incremental strains.

Vertical loading (unilateral and bilateral)s:

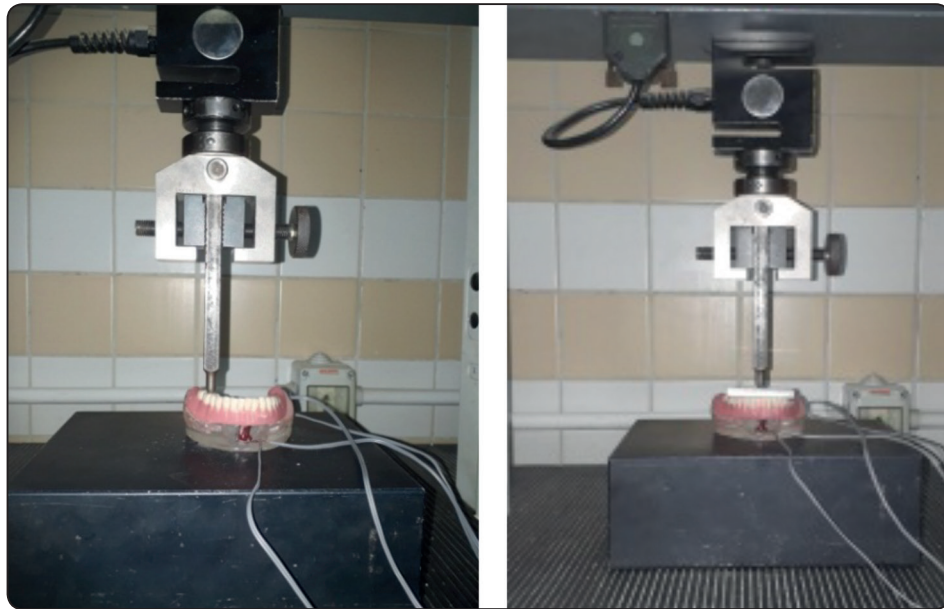
The overdenture retained by ball attachment

was seated on acrylic model . A 100 N load applied unilaterally at central fossa of right first molar, then application of metal rod on right and left first molar in central fossa).

Load application and strain recording measurement

LLOYD LR5K universal testing machine was used . The compressive load was 100 N static load, with cross head speed 0.5mm/sec and the machine was computer controlled by the NEXYGEN® software which permits the collection of dat. Numerical data were represented by mean and standard deviation (SD) values and were explored for normality by checking the data distribution, calculating the mean and median values and using Kolmogorov-Smirnov and Shapiro-Wilk tests. Data showed non-parametric distribution so; they were analyzed using Mann-Whitney U test for intergroup comparisons and Friedman's test of repeated measures followed by Dunn's post hoc test for intragroup comparisons. The significance level was set at $P \leq 0.05$ for all tests. Statistical analysis was performed with IBM® SPSS® (SPSS Inc., IBM Corporation, NY, USA) Statistics Version 25 for Windows.

* Nexygen plus materials test and data analysis software. Flexible software, allows the operator to control and monitor all aspects of the system from a single front end, ensuring fast, reliable and powerful testing and data analysis for tensile, compression, peeling, tearing, creep, relaxation and flexural test applications.



Unilateral left first molar

Bilateral Right, left molar

RESULTS

1- Comparisons of micro-strain (N) with unilateral load

Unilateral load at the Left side:

When comparing the mean microstrain recorded at each of the four surfaces ; Buccal , lingual ,right and left ,for the two attachments ,Ball and CMLOC it was founded that ,there was a statistically significant higher mean microstrain for the Ball attachment at the three surfaces ; buccal (P-value <0.001), lingual

(P-value <0.001) and left surface (P-value <0.001), except for the right surface there was no significant difference in the mean microstrain recorded between the Ball and CM LOC attachment.

The Ball attachment (391.26±111.77) have shown a statistically significant higher average microstrain than the CM LOC attachment (223.22±69.56).

2- Comparisons of micro-strain (N) with bilateral load

With bilateral load, when comparing the mean microstrain recorded at each of the four surfaces;

TABLE (1) Mean, Standard deviation (SD) values of micro-strain (N) in both groups with left unilateral load.

Direction of load	Surface of measurement	Micro-strain (mean±SD)		P-value
		CM LOC	Ball and socket	
Left	Buccal	13.44±8.54 ^C	157.72±58.87 ^C	<0.001*
	Right	179.68±102.60 ^B	224.20±129.30 ^C	0.145ns
	Lingual	532.82±222.84 ^A	809.64±373.93 ^A	<0.001*
	Left	124.77±84.08 ^B	373.47±193.09 ^B	<0.001*
	Average	223.22±69.56 ^B	391.26±111.77 ^B	<0.001*

TABLE (2): Mean, Standard deviation (SD) values of micro-strain (N) in both groups with bilateral load

Direction of load	Surface of measurement	Micro-strain (mean±SD)		P-value
		Ball and socket	CM LOC	
Bilateral	Buccal	20.83±24.99 ^C	38.45±15.99 ^B	p<0.001*
	Right	132.67±56.12 ^A	10.86±6.13 ^B	p<0.001*
	Lingual	56.00±66.25 ^{BC}	458.28±204.43 ^A	p<0.001*
	Left	217.67±116.72 ^A	568.62±256.80 ^A	p<0.001*
	Average	106.79±41.29 ^{AB}	269.05±120.39 ^A	p<0.001*

Different superscript letters within the same vertical column indicates a statistically significant difference; significant ($p \leq 0.05$) ns; non-significant ($p > 0.05$)*

Buccal, lingual, right and left, for the two attachments, Ball and CM LOC it was founded that, there was a statistically significant higher mean microstrain for the CM LOC attachment at the buccal (P-value <0.001), lingual (P-value < 0.001) and left surface (P-value < 0.001).

The mean microstrain recorded at the right side was statistically significant higher with the Ball attachment (132.67±56.12) then the CM LOC (10.86±6.13).

The CM LOC attachment (269.05±120.39) have shown a statistically significant higher average microstrain than the Ball attachment (106.79±41.29)

DISCUSSION

Discussion of Methodology:

An in vitro study rather than an invivo was selected to compare the induced microstrains because laboratory studies are more easily controlled, more practical and can yield more accurate results especially when the experiments are concerned with stress analysis. Although there is a difficulty in reproducing the physiology of the oral masticatory system, many authors used the invitro studies to compare stresses induced in the supporting structures of implant supported overdenture prostheses^(11,12).

An acrylic mandibular test model was to stimulate the clinical condition in this invitro study. (El-Abd et al., 2018, Rady et al., 2017)⁽¹³⁾. The acrylic resin was the material of choice for the construction of experimental model as acrylic resin has a modulus of elasticity very close to that of compact bone (Harder et al., 2011)⁽¹⁴⁾. This mandibular test model remained constant through out the experiment, in order to control the variables. The physical properties of acrylic resin do not simulate the complex nature of living bone, as the mechanobiology of bone and osseointegration, so the results of this study are only descriptive.

The advantages of Molloplast –B, ensured that it would remain constant throughout the experiment owing to its dimensional stability (Rady et al., 2017)⁽¹⁵⁾. A single implant retained mandibular overdentures have proved to be a cost effective simple treatment modality especially in elderly patients (Mahoorkar et al., 2016, Kanazawa et al., 2018).^(16,17) Implant success and prosthetic outcome and patient satisfaction are comparable whether one or two-implants are used for support of mandibular overdentures. In addition to cost effectiveness of the single implant overdenture, there are potential surgical advantages as well (Kanazawa et al., 2018)⁽¹⁷⁾ that was the reason a single implant installed in the mid line of a completely edentulous

mandible. The ball attachment has been used as the gold standard in this invitro study owing to its several advantages; simplicity in design, ease of use and maintenance, low cost, varying degrees of retention, wide range of movement, great patient satisfaction and used to increase retention of implant complete and partial overdenture prostheses with regard to optimizing stress and minimizing denture movement (**Cheng et al., 2012**)⁽¹⁸⁾.

The Cendres Metaux Locator (CM-LOC) attachment was recently introduced with its PEKK matrix as an alternative to the ball attachment. It is claimed that its new design and materials may significantly reduce wear and subsequently less matrix exchange and less maintenance. However, the clinical performance of this attachment regarding single implant overdenture is not tested yet (**Naguib et al., 2019**)⁽¹⁹⁾.

Unilateral and bilateral forces were applied to central fossa of the first molar of mandibular overdenture retained by implant as the first molar is considered (**Kono et al., 2014, ELSyad et al.2016, Rady and Abdel Nabi 2017**)^(20,21,22).

Discussion of results:

When comparing the mean microstrain between the ball and the CM LOC attachment when subjected to unilateral loading, it was found that the overdenture with the ball attachment have recorded a statistically significant higher mean microstrain than the overdenture retained with the CM LOC attachment, this would mainly be due to the absence of vertical resiliency of the ball attachment and also the ball and nylon matrix would contact each other without intervening space. This comes in agreement with (**ELAbd et al., 2017**)⁽²³⁾, this study concluded that high stress concentration were recorded with ball attachment on the loading side.

On contrast the CM LOC attachment has a PEKK matrix design with a slot in the matrix, this slot will expand upon loading, thus resulting in

more vertical resiliency that would allow movement of the prosthesis. During unilateral loading the overdenture have experienced a slight rotation, resulting in inducing more micro-strain to the implant when analyzing the micro-strain recorded by both types of attachment it was found that the ball attachment have induced a higher microstrain during disengagement than the CMLOC. The reason for this would be the difference in the properties of the nylon cap, and the PEKK cap. The nylon cap induce more stresses during disengagement than the PEKK which would disengage faster and so transmitting less stresses to the underlying implants. There tends to be a correlation between release period at which an attachment loses retention and the amount of stresses transferred to the abutments, the faster the attachment releases the less stress is placed on the abutments or implants.

When applying unilateral load at the left side, there was no significant difference in the mean microstrain recorded between the Ball and CM LOC attachment at the right side only while all other surfaces were statistically significant. An explanation for this would be that both attachments will tend to rotate when load around a single fulcrum line when load is applied and so would tend to disengage at the side opposite to the load applied which is the right side in this case. Still the ball attachment have recorded higher mean micro-strains when compared to the CMLOC but was not statistically significant which indicates that the CMLOC attachment would release faster than the ball attachment.

When comparing the mean micro-strain induced during bilateral loading for the overdenture retained by both attachments; the CM LOC attachment and the Ball attachment, it was found that CM LOC attachment have shown a higher statistically significant mean microstrain than the ball attachment, that is mainly due to that when loads are applied bilaterally and the CM LOC attachment

seems to disengage from one side the load on the other sides prevents such disengagement so the result will be that all stresses will be induced to the underlying implant and despite the fact of improving the stability of the denture. While for the ball attachment, it will not disengage easily, and so when loads are applied bilaterally there tends to be a rotational movement of the denture, and so less forces transmitted to the underlying implant.

CONCLUSIONS

Within the limitation of this invitro study

It can be concluded from this invitro study that the newly introduced attachment the CM LOC tends to show a better performance with regards to the micro-strains induced around the implants. On the other hand the ball attachments tends to show more micro-strain around the implants.

As there is no one attachment that would fulfill the ideal requirements, because each clinical situation is unique, so careful selection of attachment is necessary to satisfy the patient's needs and expectations, as well as establishing a long term biologic and functional result.

RECOMMENDATIONS

Further randomized clinical trials with large sample size comparing the Ball attachment and CM LOC attachment for a single implant retained overdenture, and evaluating many outcomes; patient satisfaction, quality of life, maintenance, retention⁽¹⁸⁾, in order to evaluate the performance of CM LOC attachment as the randomized clinical trials are very few for this type of attachment.

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