

Original Article

EFFICACY OF BUILD DIRECTION OF 3D PRINTING FULL COVERAGE PROVISIONAL RESTORATION ON THE MARGINAL INTEGRITY (AN IN-VITRO STUDY)

Geirges Nessim Shoukry¹, Omaila Salah eldein El Mahallawi¹, Dina Magdy El-shahawy¹

¹ Fixed Prosthodontics Department, Faculty of Dentistry, Cairo University

E-mail: geirges.nessim@dentistry.cu.edu.eg

Abstract

The aim of this study was to evaluate efficacy of build direction of 3D printing full coverage provisional restoration on the marginal integrity. The prepared resin tooth was scanned and single crown was designed using computer-aided design (CAD) software. Provisional crowns were printed using a SLA-based 3D printer at 2 directions vertical (120°) and horizontal (180°) with 16 crowns in each direction. In total, Thirty two crowns were printed. To measure the marginal gap using USB Digital microscope, then morphometric measurements were done for each shot [3 equidistant landmarks along the cervical circumference for each surface of the specimen (Mesial, buccal, distal, and lingual), and a silicone replica was fabricated for measuring internal fit, the replicas were carefully sectioned into four equal segments. From the four sections obtained from each replica, two opposite sections were used to measure internal fit, with five regions measured on each section (finish line, axial wall and occlusal), yielding 10 internal measurements for each coping and the thickness of the silicone impression material was measured using a digital microscope. It was found that horizontal group recorded statistically significant higher marginal gap mean value (44.76 µm) than vertical group (34.37 µm) as indicated by t-test ($P=0.0002 < 0.05$), considering internal fit regardless to measurement site, totally there was non-significant difference between both groups vertical group (96.042 µm) and horizontal group (91.793 µm) as indicated by two-way ANOVA test ($p=0.6179 > 0.05$) where (vertical group > horizontal group). With the limitation of this study the following conclusions could be drawn: Marginal fit of provisional restorations fabricated using a SLA based 3D printer revealed clinically accepted outcomes within the two build angles. Regarding the marginal gap, vertical orientation (120°) considered the optimal 3D printer building angle. The building angle of fabrication doesn't affect internal fit of the provisional restorations

Keywords: 3D printer, fixed prosthesis, marginal gap, exocad, CAD/CAM.

I. INTRODUCTION:

The provisional restoration is a critical phase in fixed prosthetic treatment; it is used from the time of tooth preparation to the time of final cementation. A properly fabricated provisional restoration is important in achieving a successful final restoration.

A provisional crown is a temporary (short-term) crown used in dentistry. Like other interim restorations, it serves until a final (definitive) restoration can be inserted. The provisional restoration has a role in pulpal protection, stabilization of occlusal relationships and occlusal function. Its importance increases greatly for oral rehabilitation cases that needs long term

provisionalization or when additional therapy is required before completion of the rehabilitation to protect the tooth, prevent teeth shifting, provide cosmetics, shape the gum tissue properly, and prevent sensitivity.

Many techniques are used to make temporary restorations. It began manually through direct, indirect and indirect-direct technique. However, the advances in materials and technology contributed to the introduction of CAD/CAM technique (subtractive manufacturing) and 3D printing technique (additive manufacturing). The direct technique of fabricating temporary crowns using polymethyl methacrylate (PMMA) has been frequently used for convenience and low costs of production, but it has the drawbacks of polymerization shrinkage, marginal discrepancy, and heat production. Today,

II. MATERIALS AND METHODS

This study was carried out to assess the marginal gap and internal fit of provisional crowns which were fabricated by horizontal 3D printing technique (intervention) compared to provisional crowns which were fabricated by vertical 3D printing technique (control).

According to the sample size calculation, a total of thirty-two crowns were constructed which were divided into two equal groups, sixteen samples for each group according to the technique of construction.

- Group (I): Sixteen crowns (n=16) fabricated by vertical 3D printing technique (control).
- Group (II): Sixteen crowns (n=16) fabricated by horizontal 3D printing technique (Intervention).

Dentoform model of maxillary 1st molar was prepared Figure (1) according to the following criteria: 2 mm occlusal reduction, 1.5 mm overall axial reductions. Figure (2). The prepared model was scanned using Medit T-300 scanner. Figure (3)

indirect fabrication is possible using computer-aided design/ computer-aided manufacturing (CAD/CAM), which facilitates remaking provisional crowns that were lost or fractured during long term use due to orthodontic treatment or altered vertical dimension.

The newly introduced technique 3D printing is spreading fast and various resins are used. It's an additive manufacturing (layer upon layer). It has the ability to manufacture precise prosthesis with minimal materials waste. It considers cheaper and faster than milling technique. It is passive with no force application and can produce finer details (under-cuts & better anatomy). The 3D printing methods include Stereolithography (SLA), Digital light processing (DLP), Selective Laser Sintering (SLS) and Fused Deposition Modeling (FDM).

Duplication of master die into thirty two epoxy resin dies through using silicone duplicating material Figure (4) and then divided into two equal group (n=16). Figure (5)

Provisional crowns were designed using Exocad software. Figure (6). STL file was produced and sent to Formlabs printer. Thirty two crowns were placed on a platform in the 3D printer software and rotated at 2 directions (120°, 180°) as shown in Figure (7-8) using preform software then provisional crowns were printed using the formlabs form2 printer using Next dent C&B PMMA resin material . Each specimen was photographed using USB Digital microscope. A digital image analysis system was used to measure and qualitatively evaluate the gap width. Figure (9-10). Measurement at each point was repeated five times. Internal discrepancy was measured by a replica technique. Figure (11) Each tooth was filled with light-body silicone and inserted into under a constant load (750 g) for 10 min, by means of a modified parallelometer.

III. RESULTS

Vertical Marginal Gap

It was found that horizontal group recorded statistically significant higher marginal gap mean value (44.76 μm) than vertical group (34.37 μm) as indicated by student t-test ($P=0.0002 < 0.05$) Figure (12)

Effect of measurement surface

Internal discrepancy:

Regardless to measurement site, totally there was non-significant difference between both groups as indicated by two-way ANOVA test ($p=0.6179 > 0.05$) where (vertical group $>$ horizontal group) Figure (13)



Figure (1): Prepared model



Figure (2): Silicone putty index



Figure (3): Scanning of the master die in Medit T-300 scanner



Figure (4): Silicon mold after setting

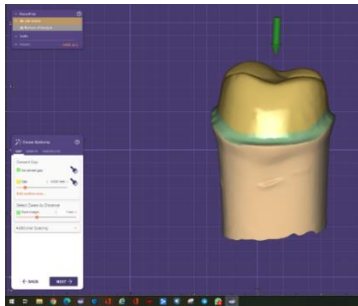


Figure (5): thirty two Epoxy resin divided into two equal group

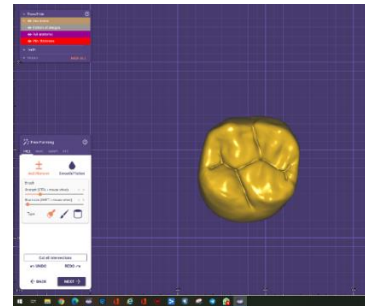


Figure (6): the final crown design ready to be saved

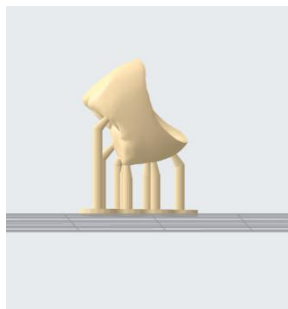


Figure (7): vertical orientation (120°)

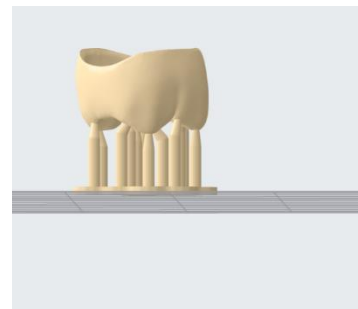


Figure (8): horizontal orientation (180°)



Figure (9) Representative microscopic image showing VM gap values for 120o group

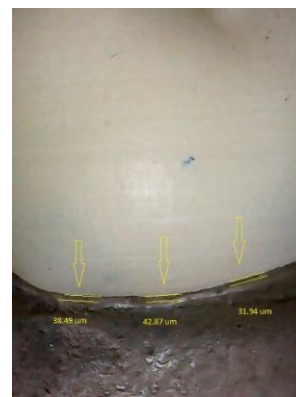


Figure (10) Representative microscopic showing VM gap values for 180o group

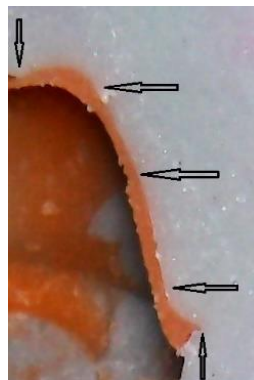


Figure (11) five regions measured in each section

IV. DISCUSSION: Recently 3D printing technology have been introduced in manufacturing of interim restorations and it has many advantages over milling subtractive technique: as it has the ability to print tiny and large objects not limited to the size of blocks as in subtractive milling technique.

This study was conducted to evaluate the effect of build directions on the marginal fit of the provisional crowns using SRT. As a result, there was a difference in the marginal fit according to build directions. Thus, the null hypothesis was rejected.

The artificial Dentoform upper right 1st molar in a model (A5AN-500, Nissin Dental Products Inc., Kyoto, Japan) was used for the aim of standardization.

In the present study, Stereolithography technique (SLA) was selected for additive manufacturing technology as it was fast with high resolution technique. The accuracy of SLA was superior to other 3D printing techniques, and it could print complex geometries with fine details.

The liquid resin used in present study was NextDent C&B biocompatible class II a material for fabrication of long term 3D printed interim restoration.

Direct view technique, through a high powerful microscope was the most commonly used method to detect marginal discrepancy. This study utilized the Digital microscope to observe marginal discrepancy, **which is a** high precision instrument that can accurately record the amount of discrepancy at various levels with remarkable precision.

Laurent et al found that if appropriate silicone is used, the cement space may be replicated and its thickness measured regardless

of the location. Similarly, **Rahme et al** reported no significant difference between the silicone replica technique and sectioning technique in measuring the marginal gap of Procera crowns and advocated that using low-viscosity silicone for the replica technique can imitate the film thickness of a cemented crown applying glass-ionomer cement

Measurements were done under a fixed magnification of 40X

Then morphometric measurements were done for each shot [3 equidistant landmarks along the cervical circumference for each surface of the specimen (Mesial, buccal, distal, and lingual). Measurement at each point was repeated five times.

There were variations in the number of points measured to assess the marginal accuracy in the previous studies. While **Nawafleh, N.A. et al** recommended 50 measurements per specimen. Others suggested that 20 to 25 measurements per specimen could be used for measuring the marginal opening. This study was conducted to evaluate the effect of build directions on the marginal and internal fit of the provisional crowns using Digital microscope (marginal gap) and SRT (internal fit).

As a result, there was a difference in the marginal and internal fit according to build directions. Thus, the null hypothesis was rejected.

In a previous study, **Abdullah et al.** evaluated a MG of provisional crowns made with 4 types of resin using low viscosity silicone impression material and reported a mean MG of 47 - 193µm.

Yao et al. reported a MG of 150 – 280µm, after fabricating provisional crowns using 4 resin types and attaching using glass ionomer cement.

Belser et al. asserted that the clinically permissible MG in the final prosthesis

was 120 μm , while **Beuer et al.** reported a range of 100 - 150 μm . In the present study, the MG was shown to be 28.18 – 65.81 μm , which falls within the clinically permissible range.

Internal fit affects the retention and resistance of the crown, in which OG is often the largest measured gap than CG or AG. According to **Boitelle et al.**, the internal fit of CAD/CAM prostheses made with various materials was 45 - 219 μm in the OG. **Alharbi et al.** reported an incisal gap of 169 μm in the 3D-printed anterior provisional crown, which was 1.5 times greater than the assigned cement gap. **Kokubo et al.** reported an incisal gap of 170 μm , which was 3 - 4 times greater than the cement gap.

In this study, the cement gap was set to be 30 μm and the measured OG was 58 - 130 μm , which was 2.5 - 5 times greater.

The AG shows a different pattern. **Alharbi et al.** reported an AG of 41 μm , which is smaller than the defined cement gap of 60 μm .

Park et al. studied 3D-printed 3-unit fixed partial dentures using resin in 5 build angles (0°, 30°, 45°, 60°, 90°) and found a significant difference in the marginal and internal fit, in which the optimal build angles were 45° and 60°, corresponding to 135° and 120° (as in our study).

Alharbi et al. compared the three-dimensional accuracy of resin crowns 3D-printed at 9 different angles using superimposition software and concluded that the optimal build angle was 120°, considering the position of support and time needed for finishing and polishing.

In addition, **Osman et al.** compared the three-dimensional accuracy of DLP-printed resin crowns and reported 135° as the optimal angle.

In this study, MG were significantly larger in the 180° group than in 120° groups. Therefore, considering the marginal gap, 120° are recommended as the optimal build angles.

Considering the internal fit Regardless to measurement site, totally it was found that **Occlusal site** recorded statistically significant highest gap mean value (115 μm) followed by **axial site** with an intermediate gap mean value (104.83 μm) while the lowest statistically significant gap mean value recorded with **marginal site** (61.926 μm) there was **non-significant** difference between both groups as indicated by two-way ANOVA test ($p=0.6179 > 0.05$) where (**vertical group > horizontal group**)

There are various reasons for the differences in the marginal and internal fit based on the build angle. First, the form of the layer created by the 3D printer differs according to the build angle. Since a SLA-based 3D printers contain a resin tank with a transparent base and non-stick surface, which serves as a substrate for the liquid resin to cure against, allowing for the gentle detachment of newly-formed layers.

The printing process starts as the build platform descends into a resin tank, leaving space equal to the layer height in between the build platform, or the last completed layer, and the bottom of the tank. A laser points at two mirror galvanometers, which direct the light to the correct coordinates on a series of mirrors, focusing the light upward through the bottom of the tank and curing a layer of resin.

The cured layer then gets separated from the bottom of the tank and the build platform moves up to let fresh resin flow beneath. The process repeats until the print is complete.

Any change in the layer form entails changes in the form and degree of polymerization shrinkage. For example, in the case of a hollow cylindrical object, there is a part that is consistently exposed to light, which affects the internal fit. Moreover, the position

of support attachment changes with the build angle. Errors can arise from the unsupported section. If support is attached close to the crown margin, then unwanted damage can be incurred during the removal of the support.

Although supports were attached symmetrically in the 180° groups, OG was significantly larger in the 120° group whose support was located more lingually. The number of supports was 12 in the 180° group and 8 in the 120° group, which explains the error in the 120° group by its relatively fewer supports.

Ji-Eun Ryu et al fabricate provisional crowns at varying build directions at 6 directions (120°, 135°, 150°, 180°, 210°, 225°) using the digital light processing (DLP)-based 3D printing and evaluate the marginal and internal fit of the provisional crowns using the silicone replica technique (SRT). And reported that The marginal and internal fit of the 3D-printed provisional crowns can vary depending on the build angle and the best fit was achieved with build angles of 150° and 180°.

Osman et al. fabricated and scanned provisional crowns in 9 different angles using a DLP-based method and obtained a color map by superimposing with original data, which showed a positive change in the internal surfaces of the supported area and the opposite area when build angles of 90°, and 270° were used. This can be explained by the gravitational effects on the liquid medium as the platform moves up and down during printing. Furthermore, CG was smaller in the 180° group than in 120° groups, while OG and AG were larger, suggesting that fit was imperfect in the axial plane.

Attempts have been made in many studies to reduce the area of support by changing the build angle. Attaching support to the object increases the printing time and the amount of material used, while removing the support requires a considerable amount of manual work and time and can degrade surface

quality. Here, the build angle is selected manually, semi-automatically or automatically.

In the manual mode, the user can directly set the build angle on the platform. In the semi-automatic mode, the angle is determined based on the feedback information on printing time and support area. In the automatic mode, it is determined by a specific algorithm that takes the printing time, as well as the amount and area of support into account.

Previous studies have proposed various algorithms to find the optimal build angle. The differences in fit after applying various algorithms must be further studied.

In this study, when the provisional crowns were printed at an build direction of 120° and 180° using a SLA 3D printer, the optimal build angles were 120°.

However, the limitation is that the cement thickness to which the crown was suitable at all angles was not set. As a result, the difference in the fit according to the position of the support was not comparable in all build angles. Also, further studies are needed to evaluate the influence of various parameters such as layer thickness, support type and location on the platform that should be considered during crown printing.

References:

1. A review. *J Manuf Mater Process* 2018;2:64.
2. Abdullah A.O, Muhammed F.K, Zheng B, Liu Y. An Overview of Computer Aided Design/Computer Aided Manufacturing (CAD/CAM) in Restorative Dentistry. *J Dent Mater Tech* 2018; 7(1): 1-10.
3. Abdullah AO, Tsitrou EA, Pollington S. Comparative in vitro evaluation of CAD/CAM vs conventional provisional crowns. *J Appl Oral Sci* 2016;24:258-63.

4. Alghazzawi TF. Advancements in CAD/CAM technology: options for practical implementation. *J Prosthodont Res* 2016;60:72-84.
5. Alharbi N, Alharbi S, Cuijpers VMJI, Osman RB, Wismeijer D. Three-dimensional evaluation of marginal and internal fit of 3D-printed interim restorations fabricated on different finish line designs. *J Prosthodont Res* 2018;62:218-6.
6. Alharbi, N, Osman, RB, Wismeijer, D. Effects of build direction on the mechanical properties of 3D-printed complete coverage interim dental restorations. *J Prosthet Dent*. 2016; 115: 760- 76
7. Ali, A.O., 2015. Accuracy of digital impressions achieved from five different digital impression systems. *Dentistry*, 5(5), p.1.
8. Astudillo-Rubio D, Delgado-Gaete A, Bellot-Arcís C, Montiel-Company JM, Pascual-Moscardó A, Almerich-Silla JM. Mechanical properties of provisional dental materials: A systematic review and meta-analysis. *PLoS One* 2018;13:e0193162.
9. Bader J, Rozier R, Mcfall W, et al: Effect of crown margins on periodontal conditions in regularly attending patients. *J Prosthet Dent* 1991;65:75-79
10. Belser UC, MacEntee MI, Richter WA. Fit of three porcelainfused- to-metal marginal designs in vivo: a scanning electron microscope study. *J Prosthet Dent* 1985;53:24-9.
11. Berman B. 3-D printing: The new industrial revolution. *Bus Horiz* 2012;55:155-62.
12. Beuer F, Neumeier P, Naumann M. Marginal fit of 14-unit zirconia fixed dental prosthesis retainers. *J Oral Rehabil* 2009; 36:142-9.
13. Beuer, F., Schweiger, J. and Edelhoff, D., 2008. Digital dentistry: an overview of recent developments for CAD/CAM generated restorations. *British dental journal*, 204(9), p.505.
14. Dawood A, Marti BM, Sauret-Jackson V, Darwood A. 3D printing in dentistry. 2015 Mar;16(1):1.
15. Dentistry. *British dental journal*. 2015 Dec;219(11):521.
16. Duke ES. Provisional restorative materials: a technology update *Compend Contin educ Dent* 1999;20:497-500.
17. Felton DA, Kanoy BE, Bayne SC, et al: Effect of in vivo crown margin discrepancies on periodontal health. *J Prosthet Dent* 1991;65:357-364
18. Frank D, Fadel G. Expert system-based selection of the preferred direction of build for rapid prototyping processes. *J Intell Manuf* 1995;6:339-45.
19. G'uth JF, Almeida E Silva JS, et al: Enhancing the predictability of complex rehabilitation with a removable CAD/CAM-fabricated long-term provisional prosthesis: a clinical report. *J Prosthet Dent* 2012;107:1-6
20. G'uth JF, Almeida E Silva JS, et al: Enhancing the predictability of complex rehabilitation with a removable CAD/CAM-fabricated long-term provisional prosthesis: a clinical report. *J Prosthet Dent* 2012;107:1-6
21. Gang-Seok Park 1, Seong-Kyun Kim 1,*, Seong-Joo Heo 1, Jai-Young Koak 1 and Deog-Gyu Seo Article, Effects of Printing Parameters on the Fit of Implant-Supported 3D Printing Resin Prosthetics, Published: 9 August 2019
22. Goodacre CJ, Bernal G, Rungcharassaeng K, et al: Clinical complications in fixed prosthodontics. *J Prosthet Dent* 2003;90:31-41

23. Güth JF, Almeida e Silva JS, Ramberger M, Beuer F, Edelhoff D (2012) Treatment concept with CAD/CAM-fabricated high-density polymer temporary restorations. *J Esthet Restor Dent* 24:310-320
24. Helena N Chia, Benjamin M Wu. Recent advances in 3D printing of biomaterials. *Journal of Biological Engineering*. 2015;9:4.
25. <https://3dprinterchat.com/design-guidelines-for-3d-printing/>
26. <https://formlabs.com/blog/3d-printing-technology-comparison-sla-dlp/>
27. <https://m.all3dp.com/2/dlp-vs-sla-3d-printing-technologies-shootout/>
28. <https://www.medit.com/dental-lab>
29. Jain, R., Supriya, B.S. and Gupta, K., 2016. Recent trends of 3-D
30. Jawahar, A. and Maragathavalli, G., 2019. Applications of 3D Printing in Dentistry—A Review. *Journal of Pharmaceutical Sciences and Research*, 11(5), pp.1670-1675.
31. Jiang J, Xu X, Stringer J. Support structures for additive manufacturing:
32. Ji-Eun Ryu, Yu-Lee Kim, Hyun-Jun Kong, Hoon-Sang Chang, Ji-Hye Jung: Marginal and internal fit of 3D printed provisional crowns according to build directions. *J Adv Prosthodont* 2020;12:225-32
33. Knoernschild KL, Campbell SD: Periodontal tissue responses after insertion of artificial crowns and fixed partial dentures. *J Prosthet Dent* 2000;84:492-498
34. Laurent M, Scheer P, Dejoux J, et al: Clinical evaluation of the marginal fit of cast crowns-validation of the silicone replica method. *J Oral Rehabil* 2008;35:116-122
35. Nawafleh, N. A., Mack, F., Evans, J., Mackay, J. and Hatamleh, M. M., 2013. Accuracy and reliability of methods to measure marginal adaptation of crowns and FDPs: a literature review. *Journal of Prosthodontics*, 22(5), 419-428.
36. Osman RB, Alharbi N, Wismeijer D. Build angle: Does it influence the accuracy of 3D-printed dental restorations using digital light-processing technology? *Int J Prosthodont* 2017;
37. Osman, RB, Alharbi, N, Wismeijer, D. Build angle: does it influence the accuracy of 3D-printed dental restorations using digital light-processing technology. *Int J Prosthodont*. 2017; 30: 182- 188
38. Pandey PM, Thrimurthulu K, Reddy NV. Optimal part deposition orientation in FDM by using a multicriteria genetic algorithm. *Int J Prod Res* 2004;42:4069-89.
39. Pandey, R., 2014. Photopolymers in 3D printing applications.
40. Park GS, Kim SK, Heo SJ, Koak JY, Seo DG. Effects of printing parameters on the fit of implant-supported 3D printing resin prosthetics. *Materials (Basel)* 2019;12:2533.
41. Paul R, Anand S. Optimization of layered manufacturing process for reducing form errors with minimal support structures. *J Manuf Syst* 2015;36:231-43.
42. Pham D, Dimov S, Gault R. Part orientation in stereolithography. *Int J Adv Manuf Technol* 1999;15:674-82.
43. photopolymer-jetting 3D printing. *J Prosthet Dent*. 2017; 118: 208- 215.
44. printing in dentistry—a review. *Ann Prosthodont Rest Dent*, 2(1), pp.101-
45. Rahme HY, Tehini GE, Adib SM, et al: In vitro evaluation of “replica technique” in the measurement of the fit of Procera crowns. *J Contemp Dent Pract* 2008;9:25-32
46. Regish, K.M., Sharma, D. and Prithviraj, D.R., 2011. Techniques of fabrication of provisional restoration:

- an overview. *International journal of dentistry*, 2011.
47. Revilla-León, M., Meyers, M.J., Zandinejad, A. and Özcan, M., 2019. A review on chemical composition, mechanical properties, and manufacturing work flow of additively manufactured current polymers for interim dental restorations. *Journal of Esthetic and Restorative Dentistry*, 31(1), pp.51-57
 48. *Scientific Dental Sciences* 3.6 (2019): 35-41.
 49. Singla, M., Padmaja, K., Arora, J. and Shah, A., 2014. Provisional restorations in fixed prosthodontics. *Int J Dent Med Res*, 1, pp.148-51.
 50. Strano G, Hao L, Everson R, Evans K. A new approach to the design and optimisation of support structures in additive manufacturing. *Int J Adv Manuf Technol* 2013;66:1247-54.
 51. Strano G, Hao L, Everson R, Evans K. A new approach to the design and optimisation of support structures in additive manufacturing. *Int J Adv Manuf Technol* 2013;66:1247-54.
 52. Tanapon Reepomaha, Onauma Angwaravong, Thidarat Angwarawong Computer-aided design/computer-aided manufacturing (CAD/CAM); 3D printing; Fracture strength; Provisional restorations. [*J Adv Prosthodont* 2020;12:218-24]
 53. Tarika M A Kohli. —3D Printing in Dentistry – An Overview. *Acta their applications in prosthodontics, a review of literature. Journal of Torabi K, Farjood E, Hamedani S. Rapid prototyping technologies and Unkovskiy A, Bui PH, Schille C, Geis-Gerstorfer J, Huettig F, Spintzyk S. Objects build orientation, positioning, and curing influence dimensional accuracy and flexural properties of stereolithographically printed resin. Dent Mater* 2018;34:324-33.
 54. van Noort R. The future of dental devices is digital. *Dent Mater* 2012;28:3-12.104.
 55. Yao J, Li J, Wang Y, Huang H. Comparison of the flexural strength and marginal accuracy of traditional and CAD/CAM interim materials before and after thermal cycling. *J Prosthet Dent* 2014;112:649-57.
 56. Zaharia, C., Gabor, A.G., Gavrilovici, A., Stan, A.T., Idorasi, L., Sinescu, C. and Negruțiu, M.L., 2017. Digital dentistry—3D printing applications. *Journal of Interdisciplinary Medicine*, 2(1), pp.50-5